



22.

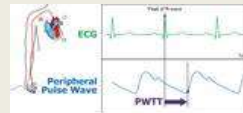
GÖĞÜS KALP DAMAR ANESTEZİ VE
YOĞUN BAKIM DERNEĞİ

ULUSAL KONGRESİ

Elimizdeki monitorizasyon gereçlerinin sınırlamaları

Doç.Dr.Şaban Yalçın, DESA
Kayseri EAH

Hemodinamik monitörler



EsCCO

EKO

USG

Flotrac

PiCCO

ÖD





© JAXA/NHK

DR. JEKYLL and MR. HYDE



ideal monitorizasyon araci



vs.



Sunu Planı

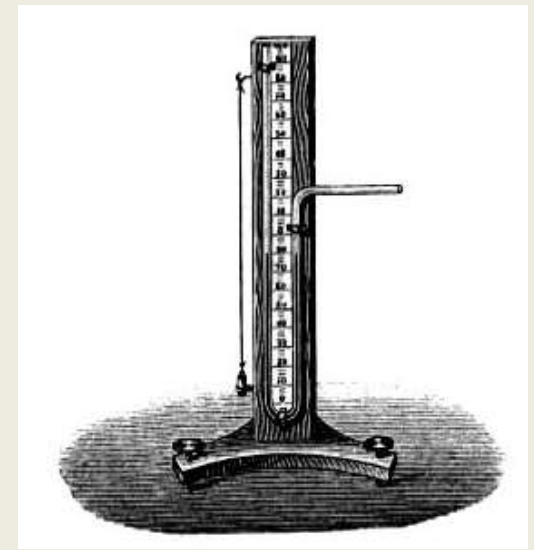


Tarihçe

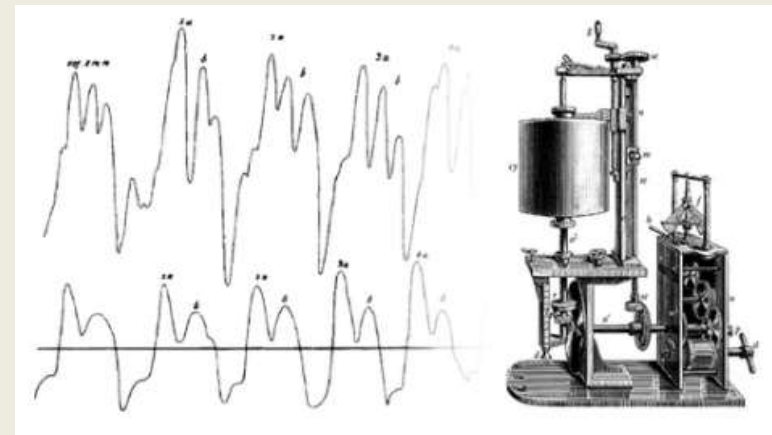
Yöntemler ve
Limitasyonları



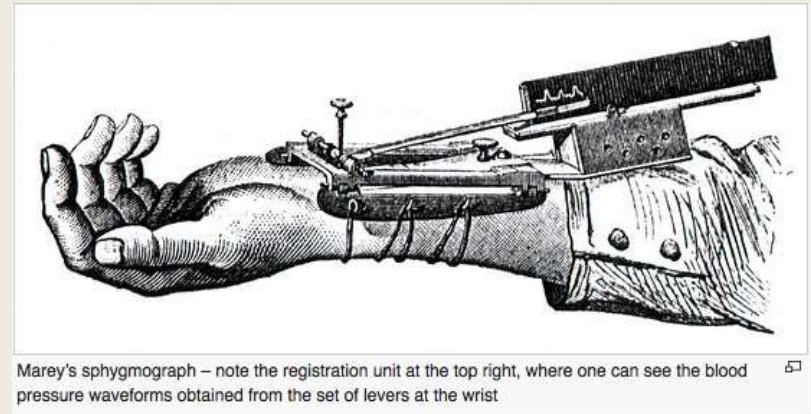
1773 Stephen Hales



1828 Jean Leonard Poiseuille



1847 kymograf Carl Ludwig



Marey's sphygmograph – note the registration unit at the top right, where one can see the blood pressure waveforms obtained from the set of levers at the wrist

“

The discovery of blood pressure was more important than the discovery of blood.

— Johannes Müller

Yöntemler

PAK,TPTD

NKA(PCA)

Doppler

Bioimpedans
Bioreaktans

PWTT

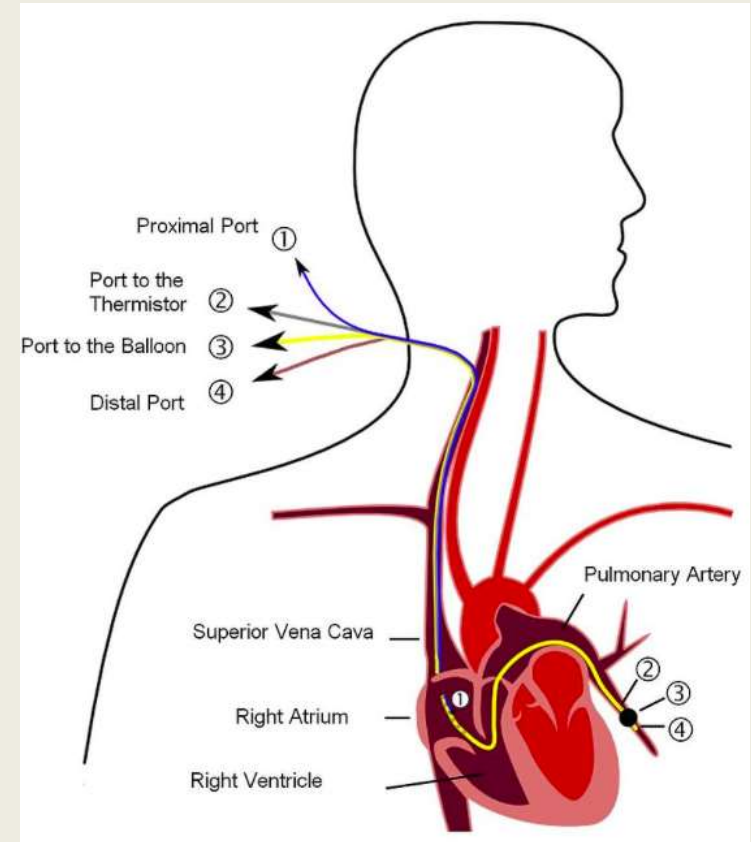
Pulmoner arter kateteri

Adolf Fick

Stewart indikatör dilüsyon

Fegler termodilüsyon

Morbidite ile ilişkili



Limitasyonlar

İndikatör kaybı (enj.öncesi-sırasında-sonrasında)

Isı volüm

Resirkülasyon

Hastanın pozisyon-cerrahi

Limitasyonlar

Vücut ısı deęişkenlięi

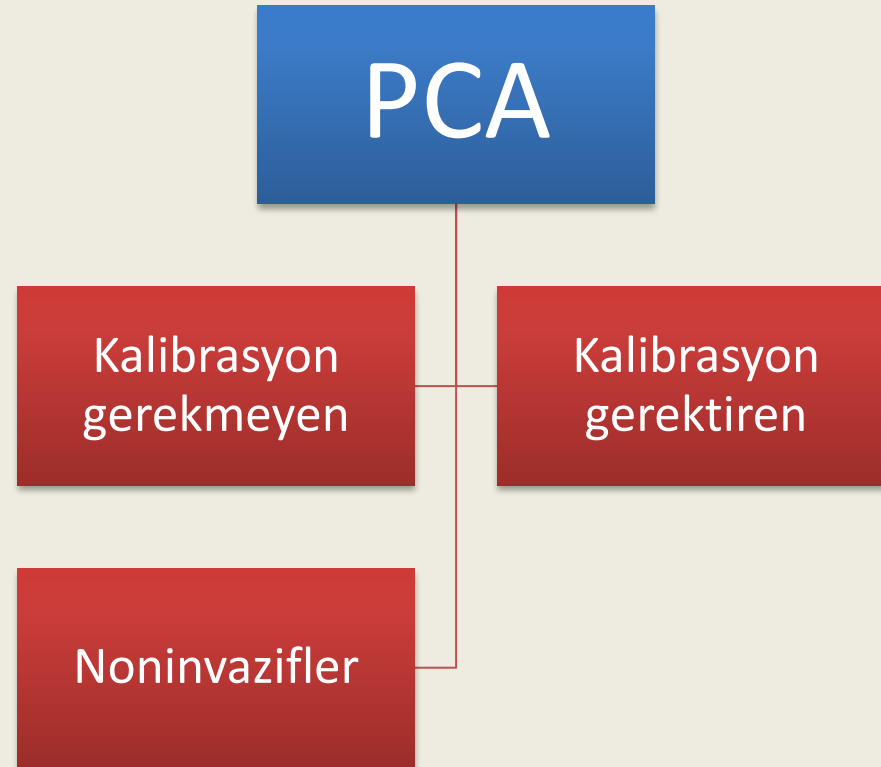
Saę kalp outputu

İnvazif-Komplikasyon

Tekrarlanabilirlik (%22)

Devamlı ölçüm yapanlarda-gecikme

Nabız kontür analizi (Pulse contour analysis)



Kalibrasyon gerektirenler (Transkardiyopulmoner termodilüsyon ve lityum)

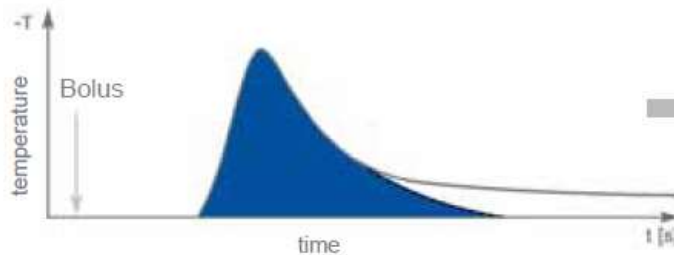
Cihaz	Kalibrasyon	Algoritm	Özellik	Dezavantaj
Lidcoplus	Lityum TPD	PulseCO	Arter morfoloji değişikliklerine az hassas	Biraz daha invazif
PiCCO	TPD	Pulse kontür analiz eder, aortik kompiyansa bölerek eğrinin sistolik kısmının alanı ile entegre eder.	Arteryal kompiyans,SV R Gerçek zamanlı KO, PAK ile karşılaştırılmış	Biraz daha invazif Hipotermi? Kalibrasyon ?
VolumeView/E1000	TPD	Langewouters	Hiperdinamik, vazoplejik hastalarda geçerli	Biraz daha invazif

Transpulmonary thermodilution



Calibration

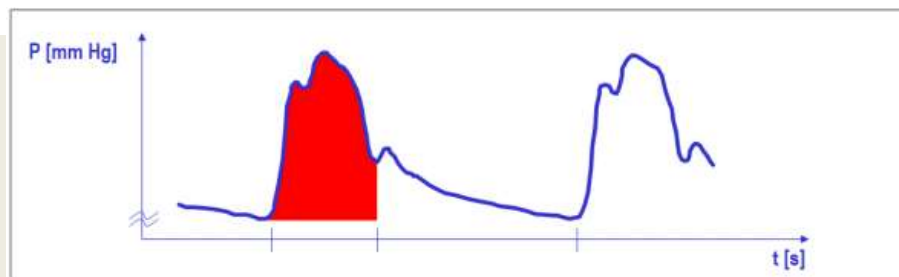
Pulse contour analysis



Cardiac output calculation:
Area under the thermodilution curve

$$CO_{TDA} = \frac{(T_b - T_i) \times V_i \times K}{\int \Delta T_b \times dt}$$

T_b = Blood temperature
 T_i = Injectate temperature
 V_i = Injectate volume
 $\int \Delta T_b \times dt$ = Area under the thermodilution curve
 K = Correction constant, made up of specific weight and specific temperature of blood and injectate



$$PCCO = cal \cdot HR \cdot \int_{\text{Systole}} \left(\frac{P(t)}{SVR} + C(p) \cdot \frac{dP}{dt} \right) dt$$

Patient-specific calibration factor (determined by thermodilution)

Heart rate

Area under pressure curve

Aortic compliance

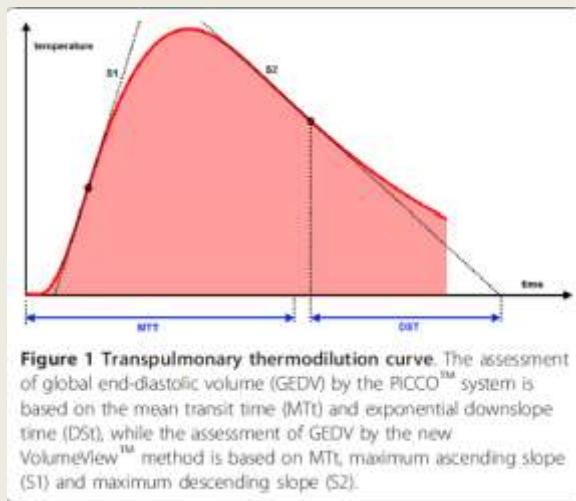
Shape of pressure curve

Transpulmonary thermodilution



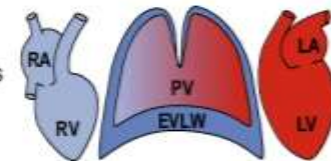
Calibration

Pulse contour analysis



1. Intrathoracic Thermal Volume: $ITTV = CO \times MTt$

Definition: Thermal distribution volumes of cardiac chambers plus pulmonary thermal volume



2. Pulmonary Thermal Volume: $PTV = CO \times Edt$

Definition: Thermal distribution volume of the lungs including intravascular, interstitial and alveolar volumes

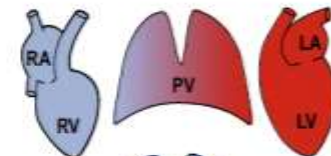


3. Global End-diastolic Volume: $GEDV = ITTV - PTV$

Definition: Sum of the end-diastolic volumes of all heart chambers, excluding intrathoracic blood volume



4. Intrathoracic Blood Volume: $ITBV = GEDV \times 1.25$



5. Extravascular Lung Water: $EVLW = ITTV - ITBV$

Definition: Water content outside of the pulmonary vasculature including the pulmonary interstitium plus any alveolar fluid



Limitasyonlar

Daha az invazif ama sađ kalple ilgili veriler yok

Mikst venöz O₂ saturasyonu yok

Çocuklar için aralıklar uygun deđil

Isı, Volüm, İndikatör kaybı, ekstrakorperyal dolaşım, TAV,
Pnömenotomi

Arter, Damping...

Limitasyonlar

Lityum tedavisi

Lityum birikimi

<40 kg

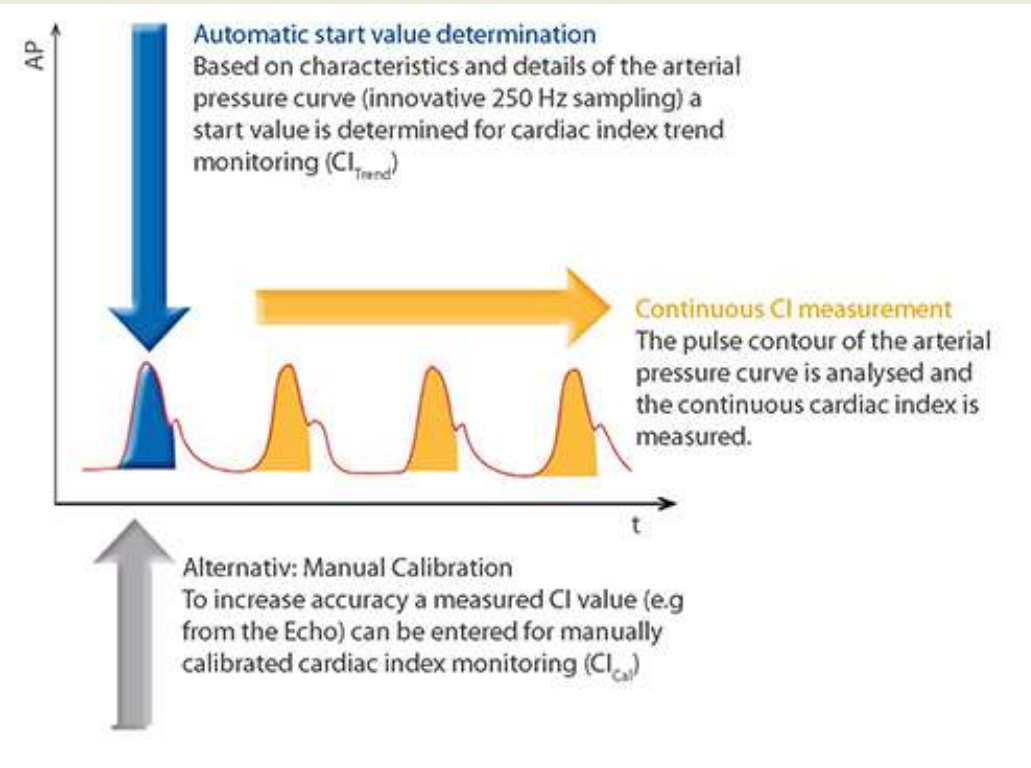
İlk trimestr

Kas gevşeticiler

Kalibrasyon gerekmeyen az invazifler

Cihaz	Algoritm	Özellik	Dezavantaj
Flotrac/Vigileo	Langewouters	En çok çalışma yapılan, Perioperatif dönemde güvenilir	Vazomotor ton Operasyon odası dışında
Lidcorapid	PulseCO	Boy, yaş, ağırlık normogramları	
ProAQT/pulsiofle x	Boy, yaş, ağırlık, MAP, HR ile otokalibrasyon	Dalga boyu analizi 250/sn	

ProAQT



Flotrac/Vigileo

The FloTrac System Algorithm

Formula for Cardiac Output = Heart Rate x Stroke Volume

FloTrac System Cardiac Output = Pulse Rate x [std(BP) * χ]

Pulse Rate [PR]

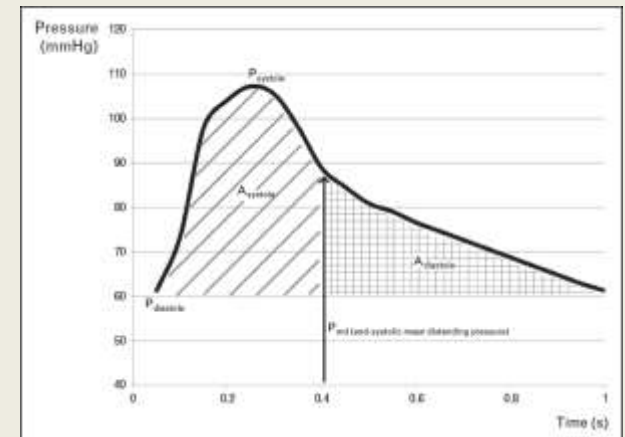
- Measured as beats per minute
- Beats identified by upslope of waveforms
- Advanced beat detection differentiates fully perfused beats
- Computed from 20-second time period of beats

Standard deviation of arterial blood pressure [std(BP)]

- Pulse pressure \propto SV \propto std(BP)
- Measured as mm Hg
- Computed on a beat-by-beat basis

The χ factor compensates for differences in vascular compliance and resistance

- Patient-to-patient differences estimated from biometric data
- Dynamic changes estimated by waveform analysis (skewness, kurtosis, of the waveform)
- Measured as mL per beat/mm Hg
- 1-minute average updates



Limitasyonlar

Algoritmeler

Damping (over-under) rezonans

Aritmi

Vasküler tonus değişikliği (NE)

iABP

Limitasyonlar

AY

Perifer arter – arteryal dalga form paterni

Ameliyatlarda

Farklı hasta grupları

Non invazif nabız kontür analizi

Volüm klemp yöntemi

- CNAP, Nexfin, ClearSight

Radyal arter applanasyon tonometrisi

- T-Line

Volüm klemp yöntemi

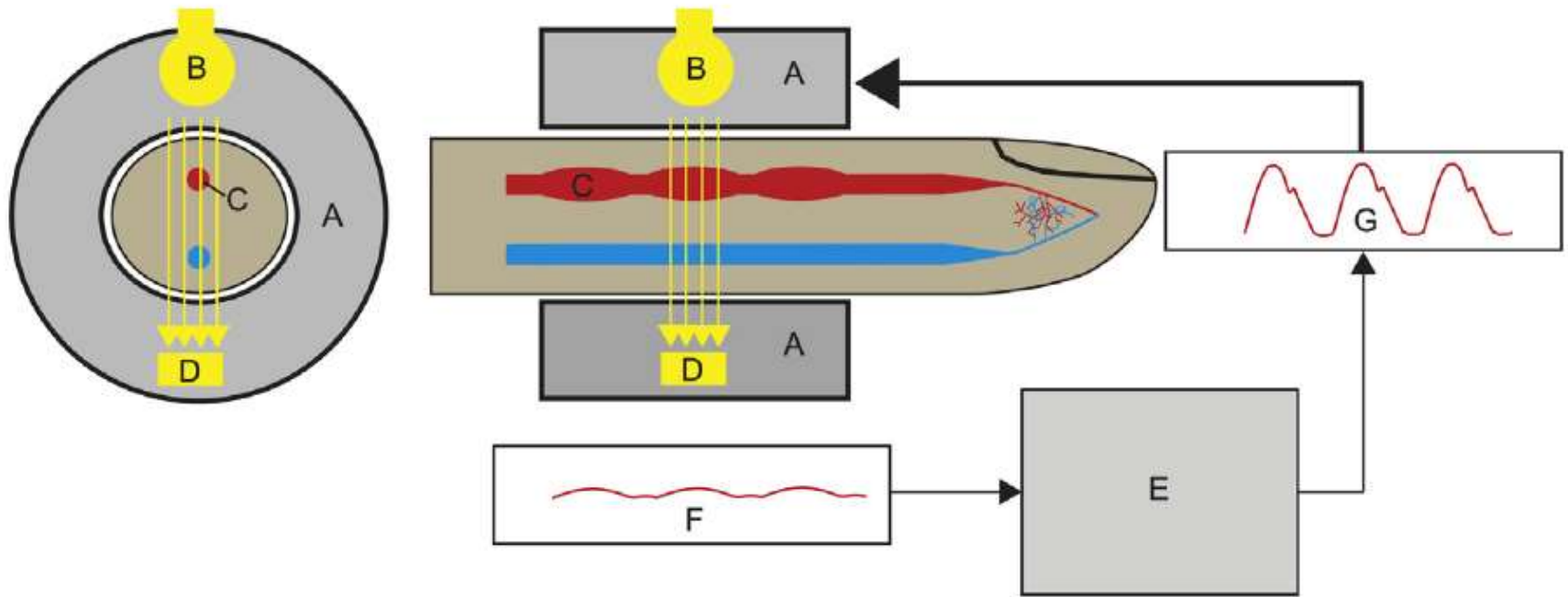
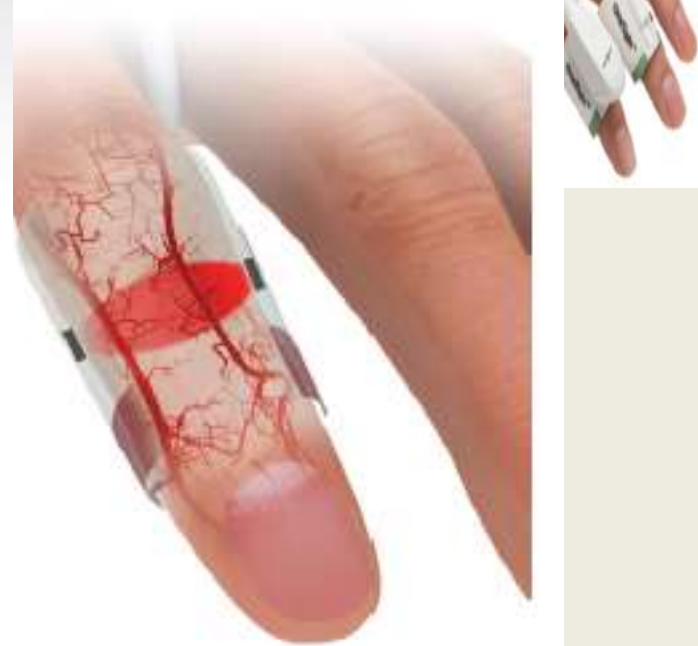


Fig. 3. Schematic illustration showing the theoretical principle of the volume clamp method (also called vascular unloading technique). An inflatable finger cuff (A) applies pressure to the finger and contains an infrared transmission plethysmograph (B) to measure the finger artery's (C) diameter (i.e., blood volume). A light detector (D) that is also integrated in the finger cuff measures the absorption of the infrared light. An increase in artery size because of an increase in blood volume (and subsequently pressure) automatically leads to an increase in cuff pressure with the help of a photo-plethysmographic control system (E) in order to keep the artery diameter constant (and the arterial wall 'unloaded'). Thus, from the pressure needed to keep the volume in the finger artery constant (F) throughout the cardiac cycle, the arterial blood pressure waveform can be derived indirectly (G).

Volüm Klemp yöntemi



Radyal arter aplantasyon tonometrisi

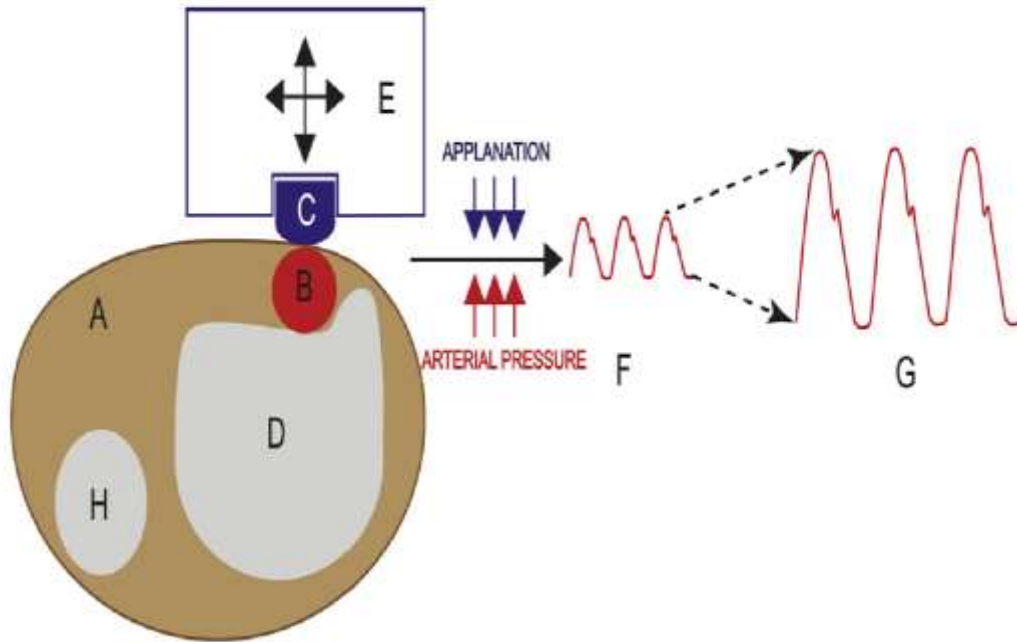


Fig. 4. Cross section of the wrist (A) with a schematic illustration showing the radial artery applanation tonometry technology. The applanation tonometry requires that the radial artery (B) be flattened (applanated) underneath a sensor (C) and be supported by a bony structure (e.g., the radius (D)). The sensor is integrated in a bracelet (E) that also holds the motors to move the pressure sensor laterally for identifying the site of maximum pulsation and up and down for achieving the optimal artery applanation. The maximum pulse pressure (equivalent to the mean blood pressure) can be obtained when the transmural pressure is zero (representing the maximum compliance of the arterial wall). Continuous non-invasive beat-to-beat recording of the arterial blood pressure waveform can thereby be derived (F). Subsequently, the arterial blood pressure waveform is scaled using proprietary signal processing algorithms based on biometric data (G). The ulnar bone is indicated by H.

Limitasyonlar

Algoritmeler

Aritmi

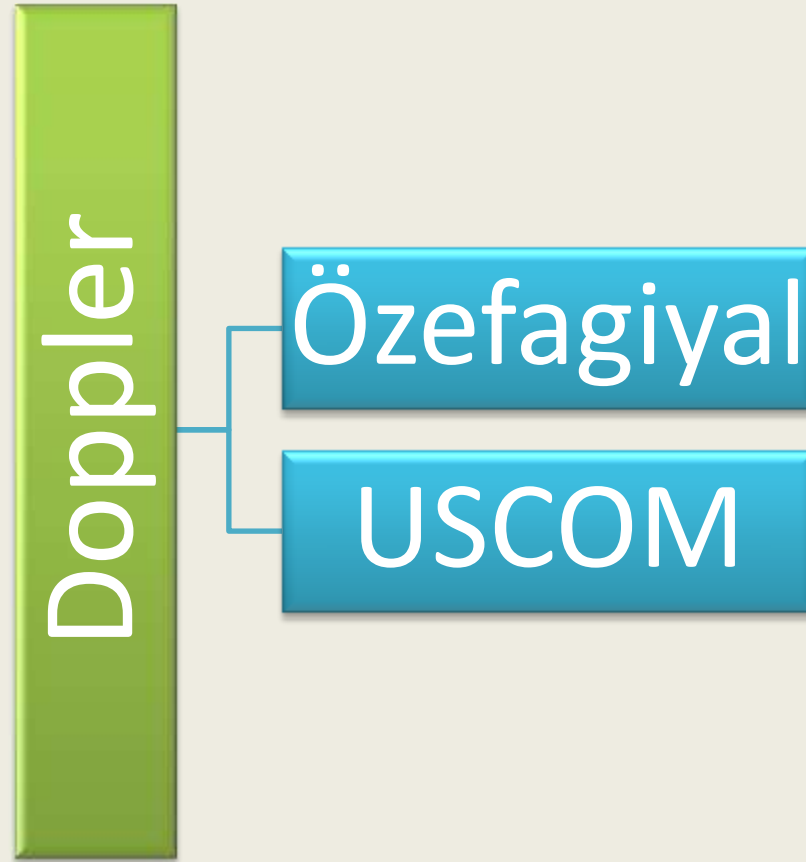
Vasküler tonus deęişiklięi

Hareket artefaktı, Sensör dislokasyonu, Parmak ödemi

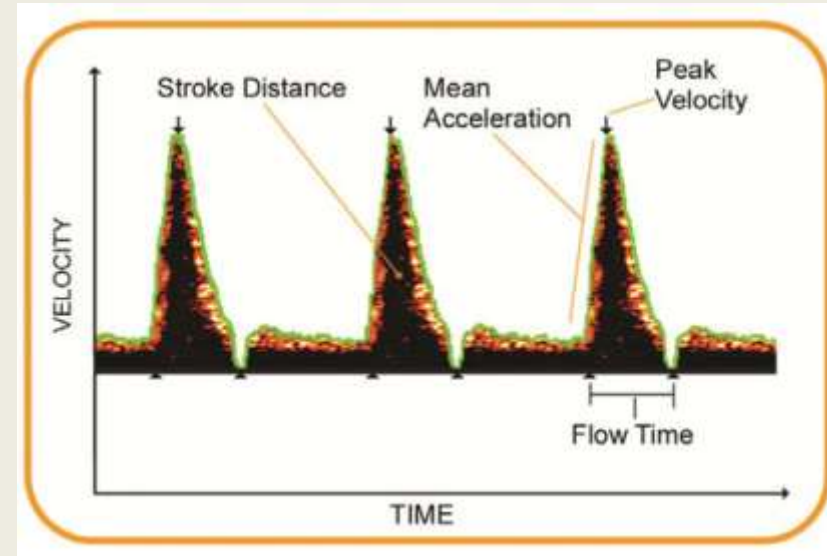
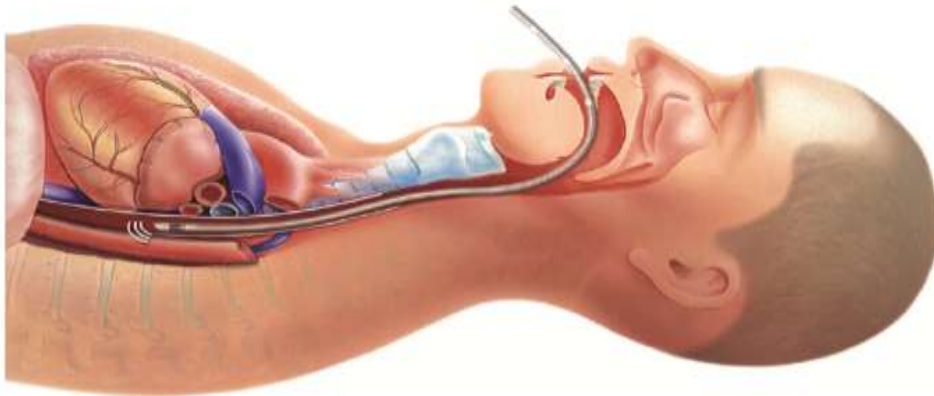
SVR, KO yüksek veya düşük

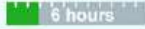

Neyi neyin yerine koymak lazım?

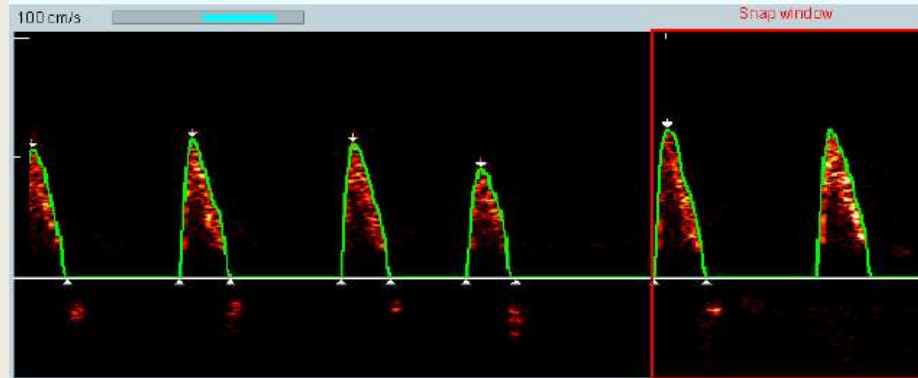
Doppler Teknikleri



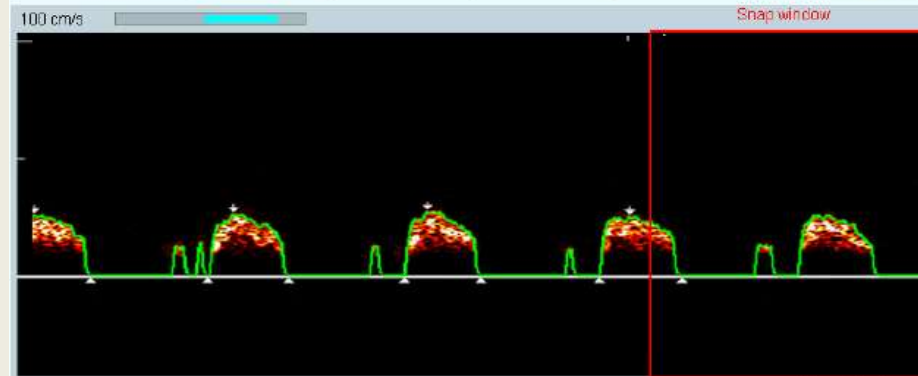
Özefagiyal Doppler EKO

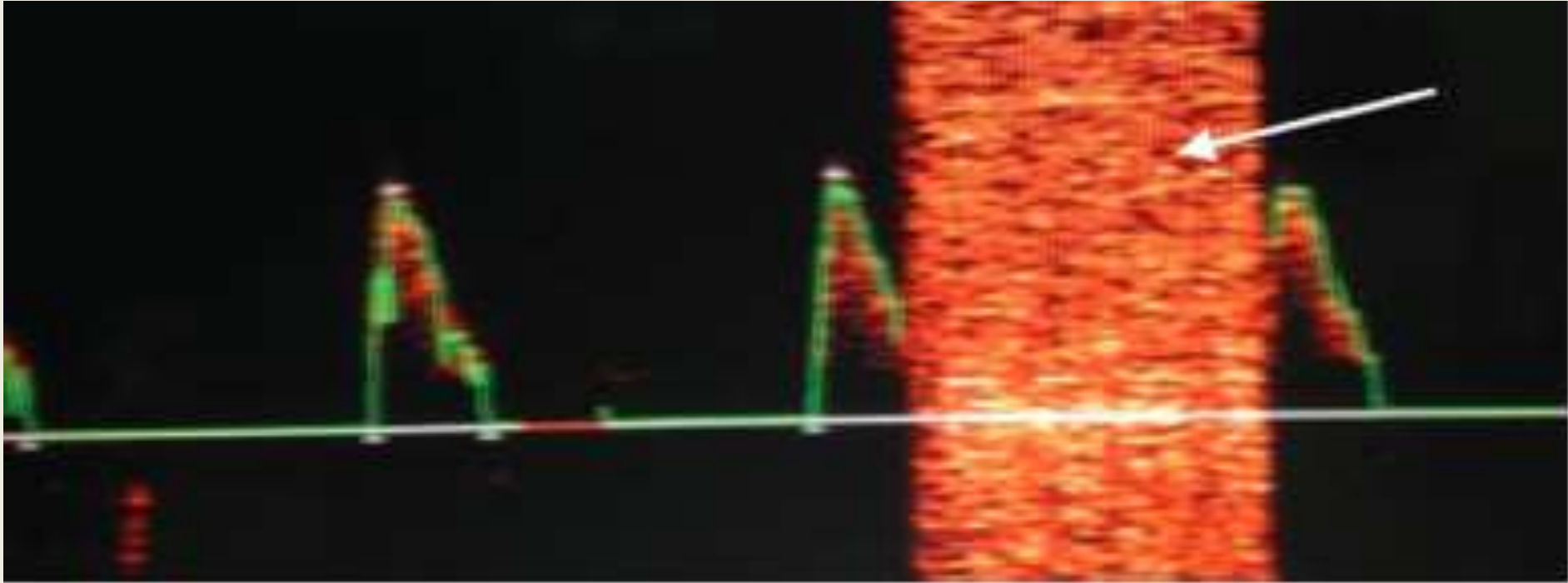


PATIENT DATA #19.12.08-11.30 Female - 68 yrs 75 kg (166 lb) 167 cm (66 in) ADULT BSA = 1.85 m ²	CO	l/m	SV	ml	FTc	ms	SD	cm	Fri Dec 19, 2008 11:30 I2S probe  Average 5 cycles Filter OFF Gain 
	3.6		39		256		4.3		
			HR	bpm	PV	cm/s			
			91		55.5				



PATIENT DATA #22.12.08-13.30 Female - 62 yrs 72 kg (158 lb) 149 cm (59 in) ADULT BSA = 1.66 m ²	CO	l/m	SV	ml	FTc	ms	SD	cm	Mon Dec 22, 2008 13:30 I2S probe  Average 6 cycles Filter OFF Gain 
	2.9		40		363		4.5		
			HR	bpm	PV	cm/s			
			73		26.1				





Limitasyonlar

Semi-invazif, Uyanık hasta?

Eđitim-Optimal sinyal elde etme

Desendan aorta-Sefal-Kaudal kan oranını ve Aortun kesitsel alanını sabit kabul eden algoritma

Aortun apı-normogram Akımı laminer kabul ediyor. Trblan?

Anevrizma, koarktasyon, IABP

USCOM



Limitasyonlar

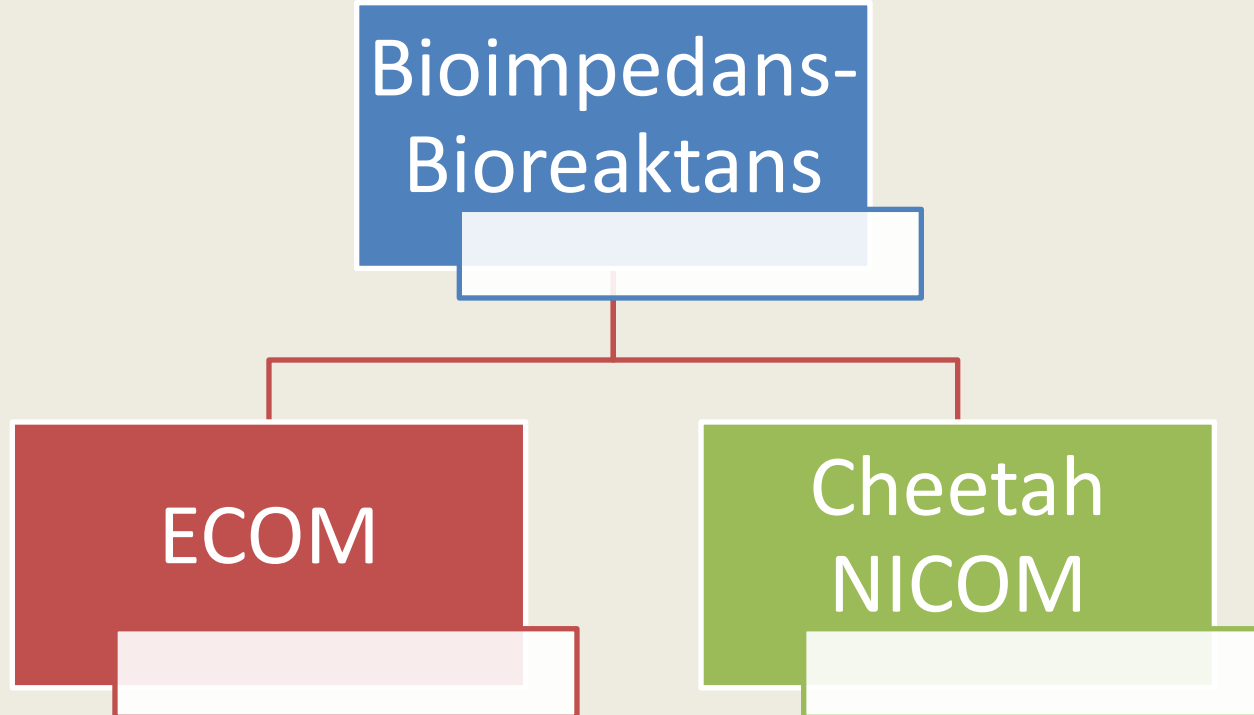
Algoritma hasta boyuna göre

Ağırlık, VYA dikkate alınmıyor

Doppler teknikleri? PW-CW

Eğitim

Bioimpedans Bioreaktans ölçümleri



Cheetah NICOM

NICOM Completely Noninvasive Cardiac Output Monitor

Cheetah NICOM provides continuous, non invasive, hemodynamic insight, delivering real time tracking of Cardiac Output and other key Hemodynamic Parameters.



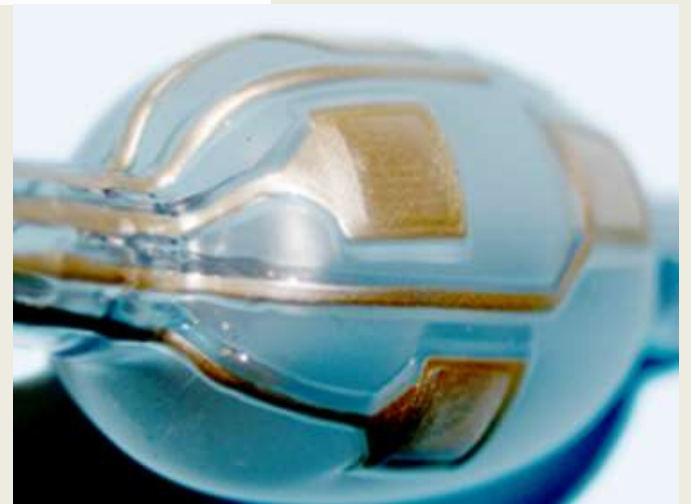
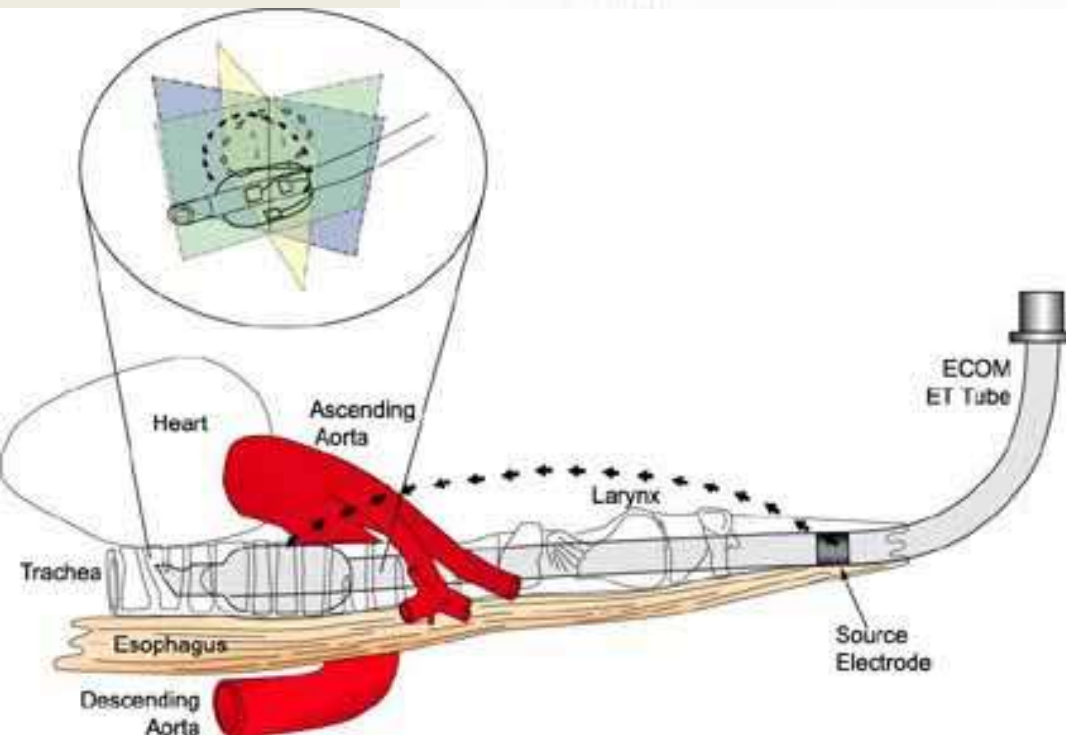
Prewired sensors



Prewired sensors and bag



Records software



Limitasyonlar

Büyük sıvı şiftleri

Pulmoner torasik patolojiler

Pulmoner ödem efüzyon

Şant

Ybc cisim (göğüs tüpü, tel, metal)

Limitasyonlar

Hareket artefaktı

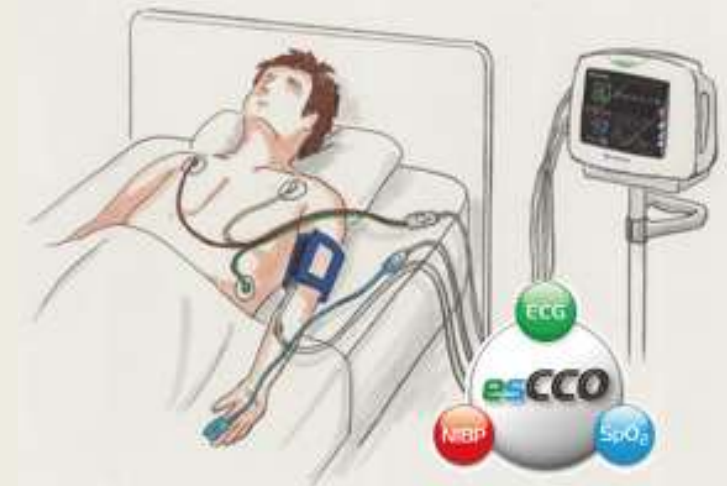
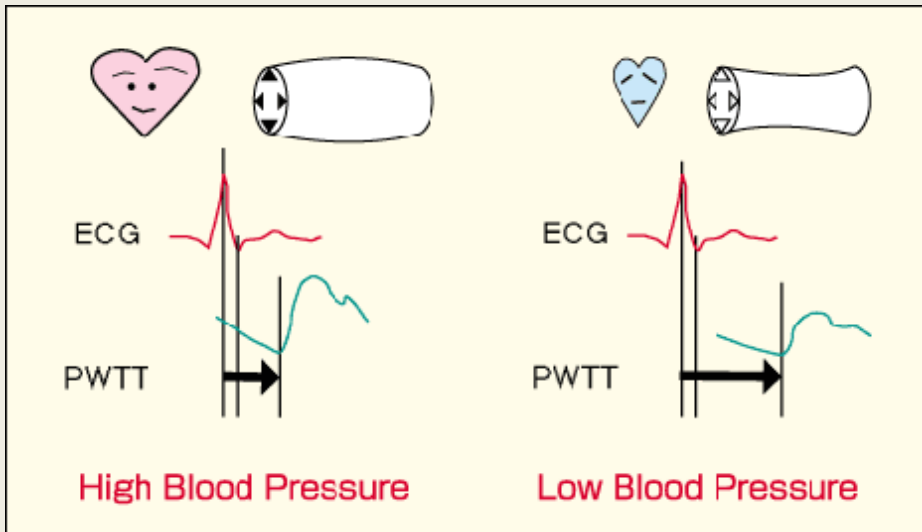
Kafın pozisyonu

Farklı hasta grupları

Çocuk için elektrot

Ne kadar gerçek zamanlı?

Nabız dalgası gecikme zamanı (PWTT)



$$CO = K \times (\alpha \times PWTT + \beta) \times HR = esCCO$$

Limitasyonlar

Başlangıçta kalibrasyon

Hemodinamik stabilite 3 dk.

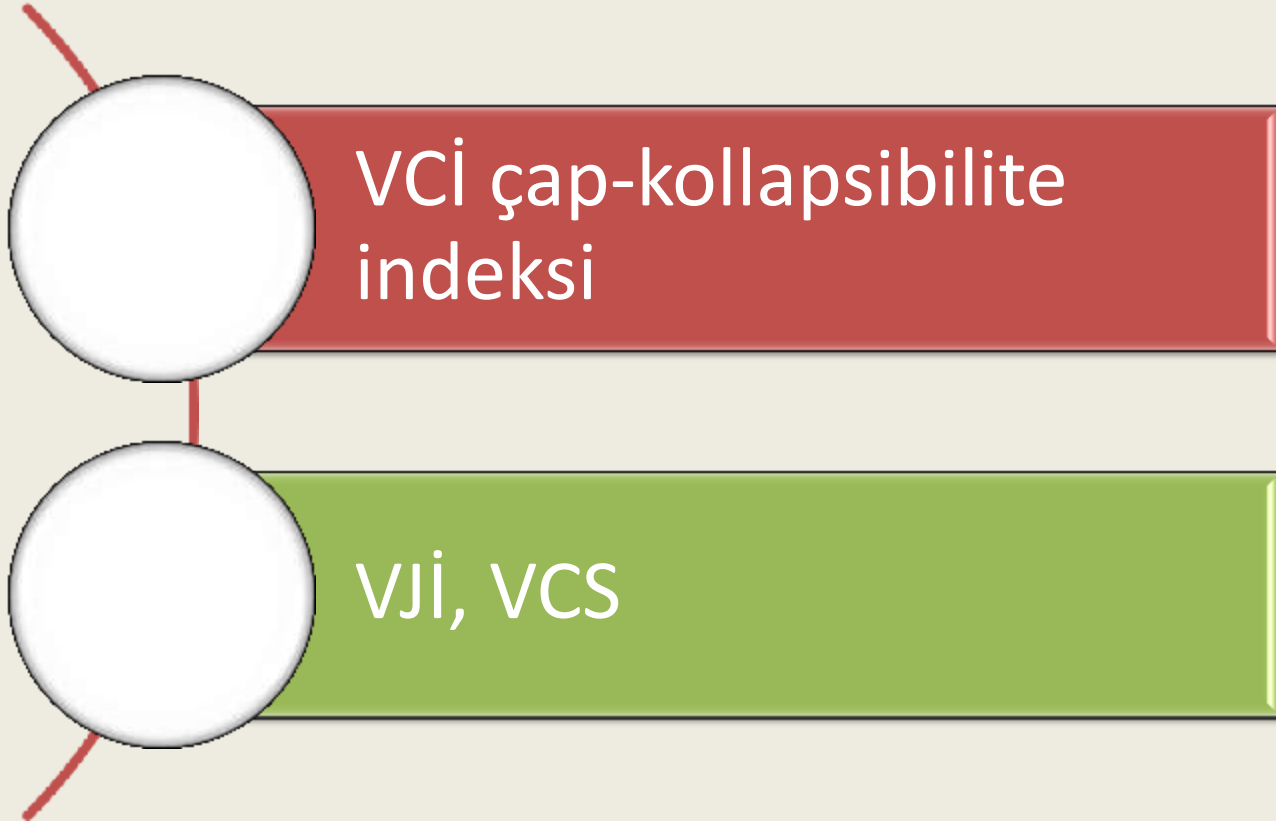
Yeni versiyon morfometrik ölçümler

Aritmi, Pacemaker, IABP

Pulse oksimetre (Hipotermi, soğuk çevre)

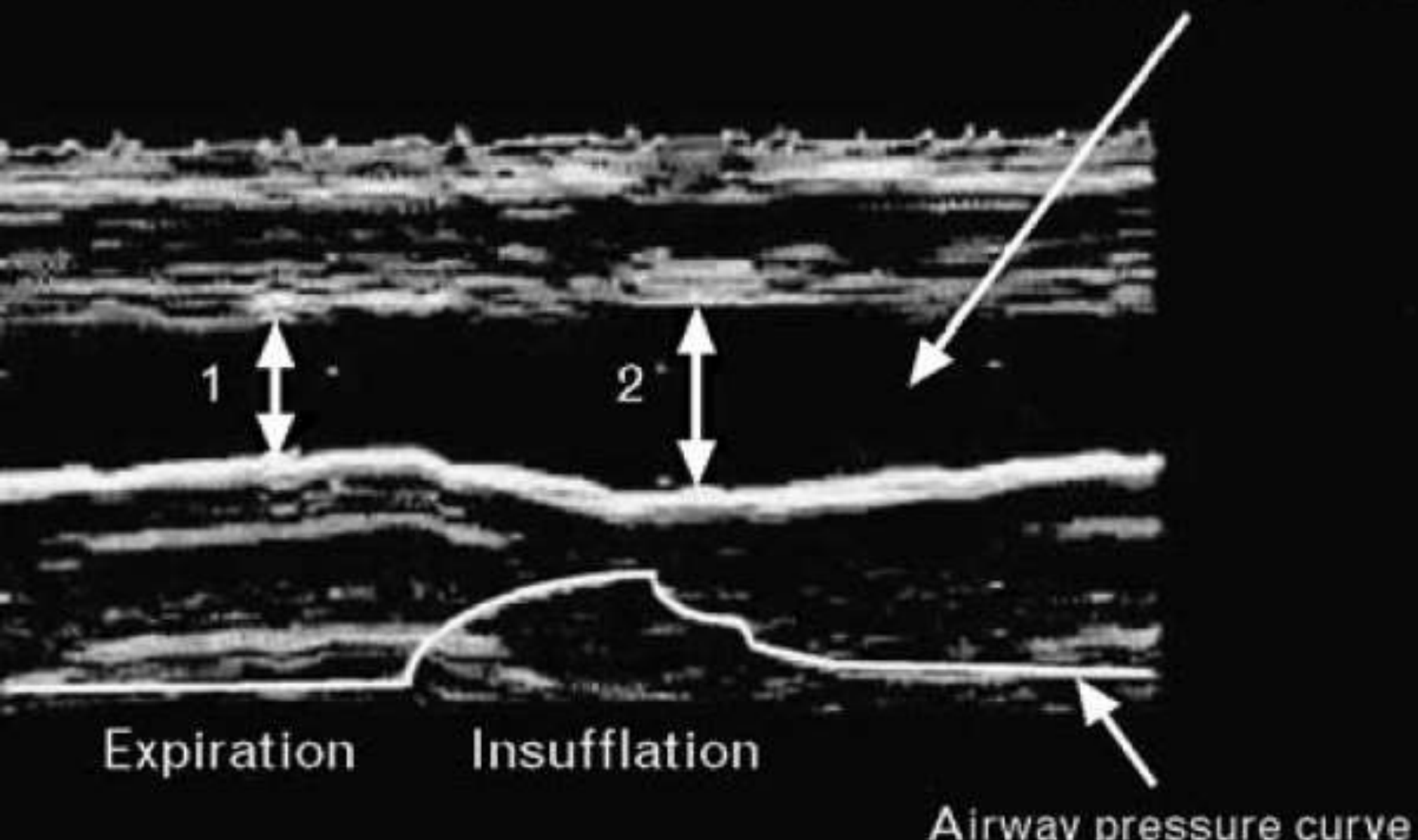
Kritik hastalar

Ultrason



1 = minimum D_{IVC}
2 = maximum D_{IVC}

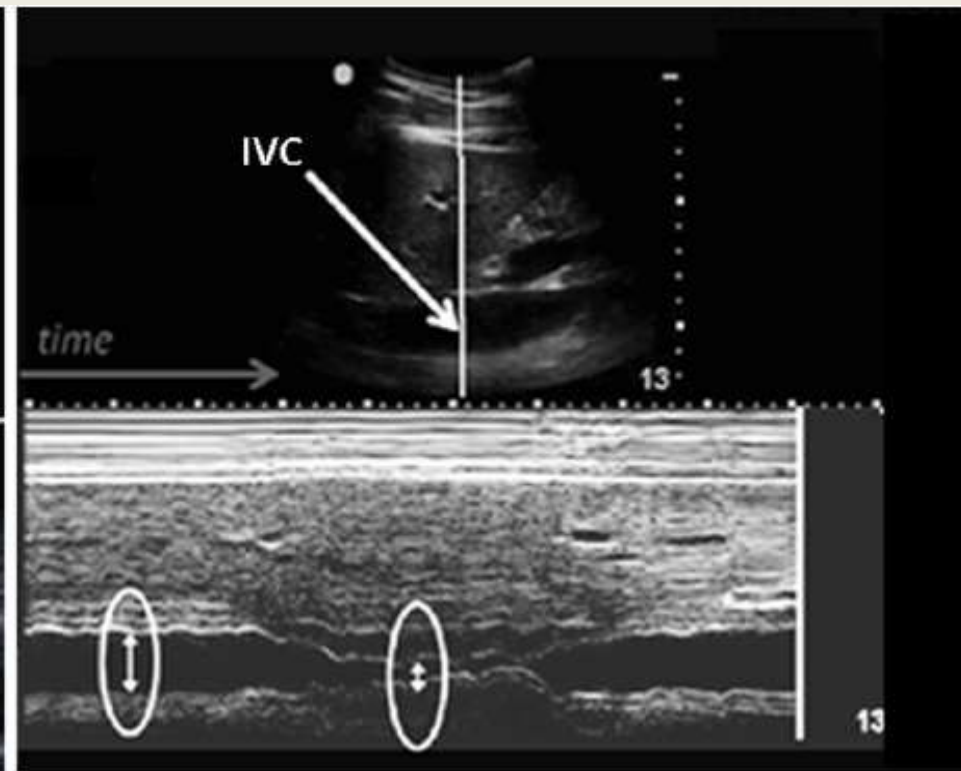
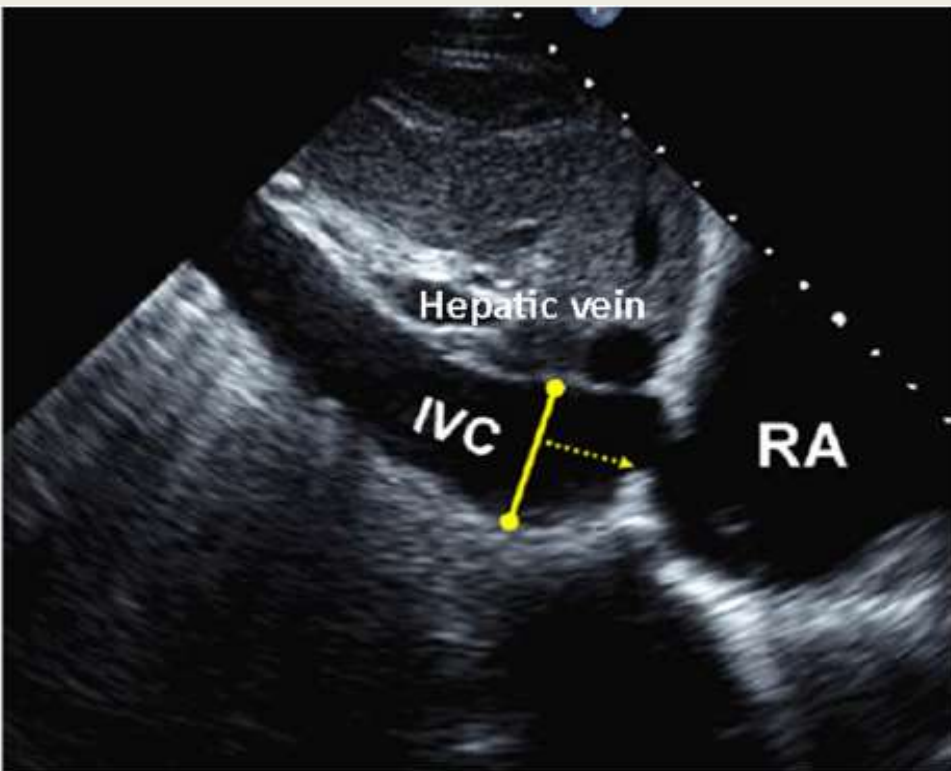
Inferior vena cava



Expiration

Insufflation

Airway pressure curve

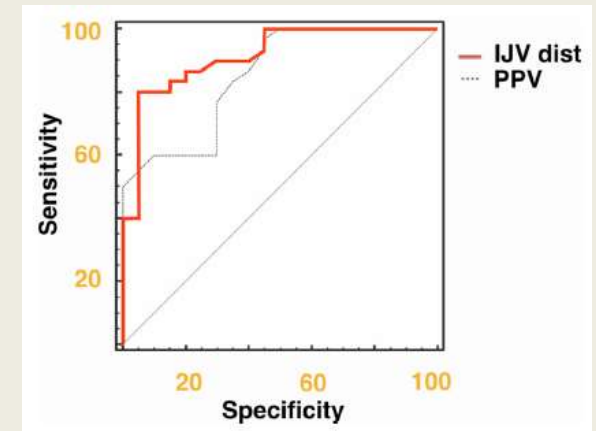
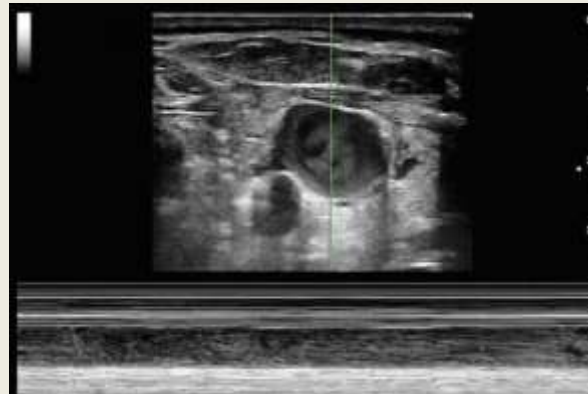
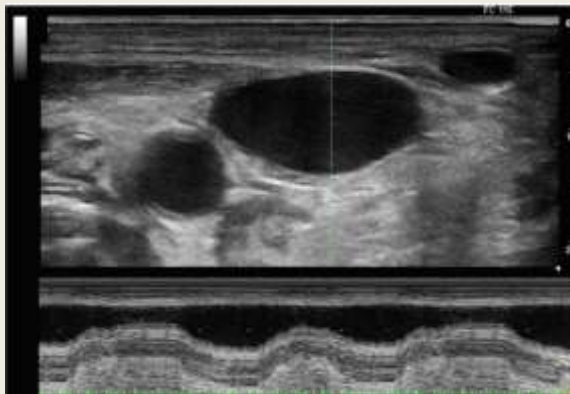


IVCi-IVCe/IVCi

RESEARCH

Open Access

Jugular vein distensibility predicts fluid responsiveness in septic patients



Limitasyonlar

Pozisyon, Solunum, Diyafram Hareketi, Prob (B line)

Kişi bağımlı

İntraabdominal hipertansiyon

Devamlı?

Ekokardiyografi



Limitasyonlar

Tecrübe

Uygulayıcı farklılığı

Hiperinflasyon, akciğer enfeksiyonları, insizyonlar, drenaj, yetersiz hasta pozisyonu

Sıvı cevabının deęerlendirilmesi

Kim Cevap Verir?

Kim Cevap Vermez?

Her cevap verene sıvı verelim mi?

Ne zaman Duralım?

Vazoaktif ajan ?



Statik
parametreler

Dinamik parametreler



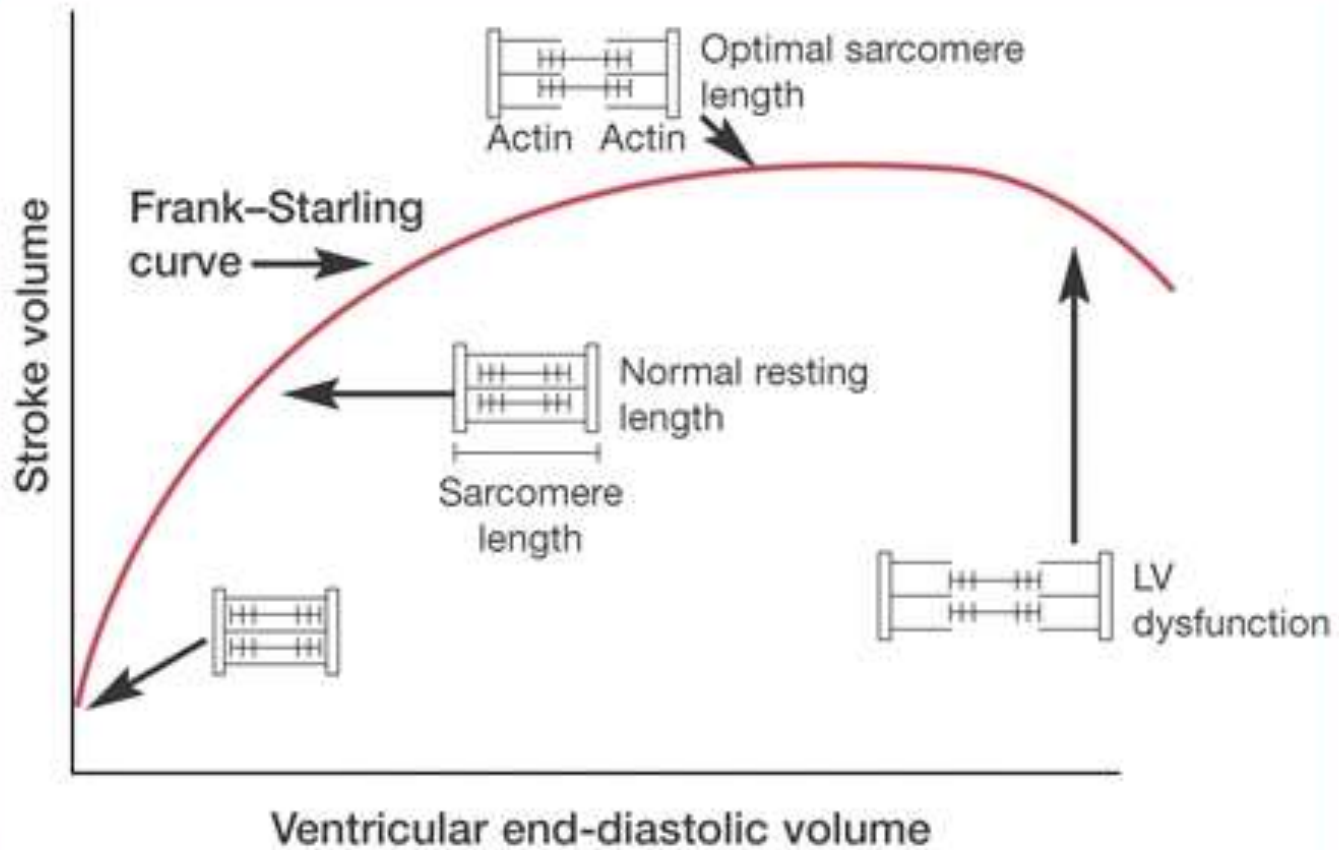
SVV, PPV, SBV

PVi

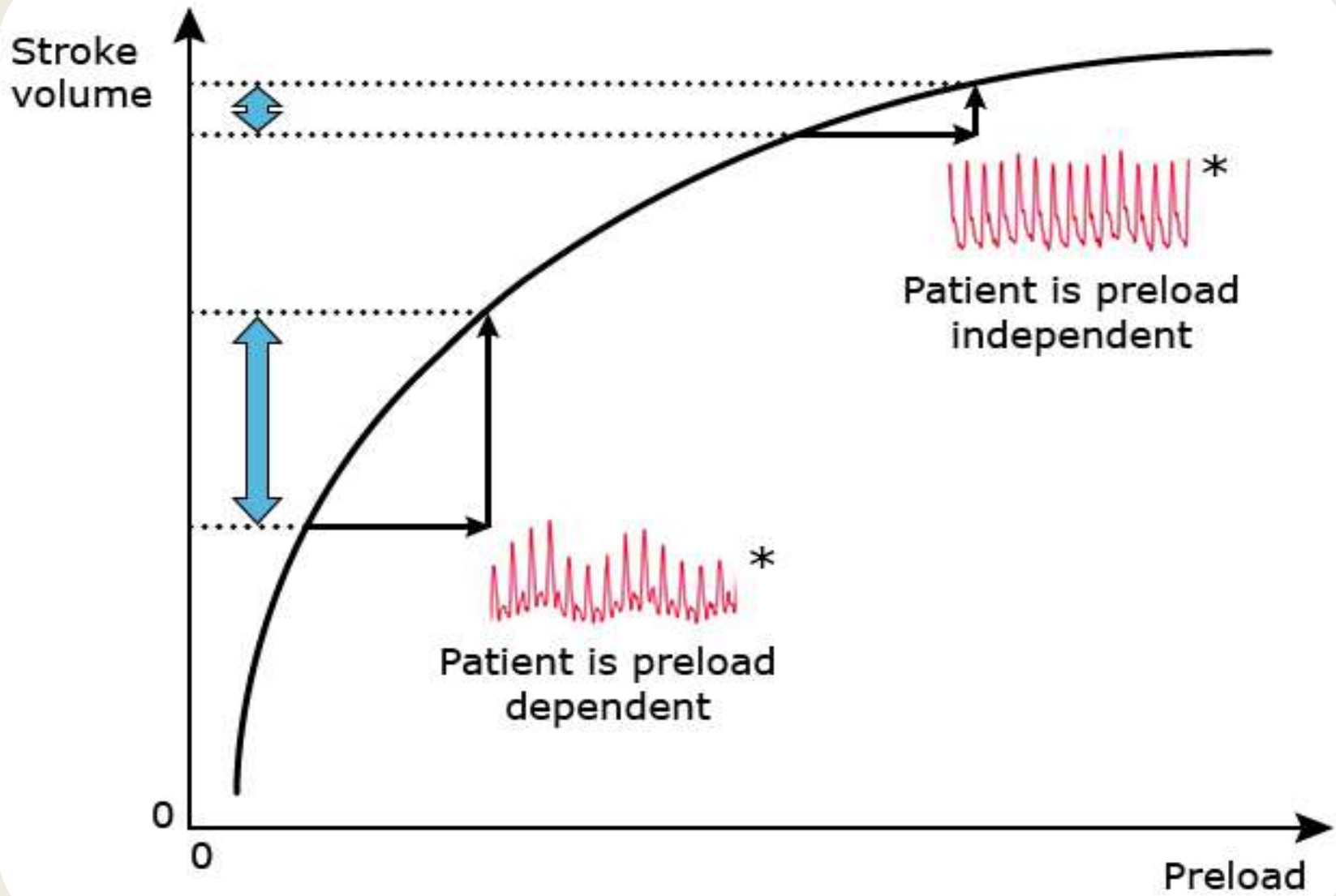
EKO (VTi-Kan velositesi)

USG (Vci-Vji)

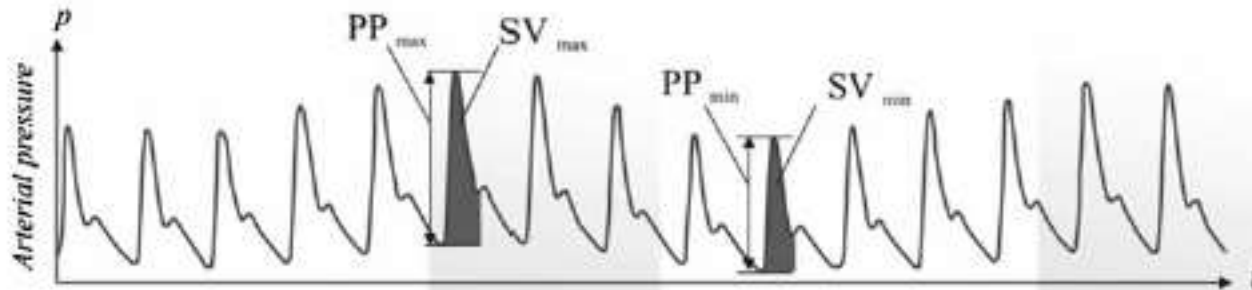
Frank-Starling



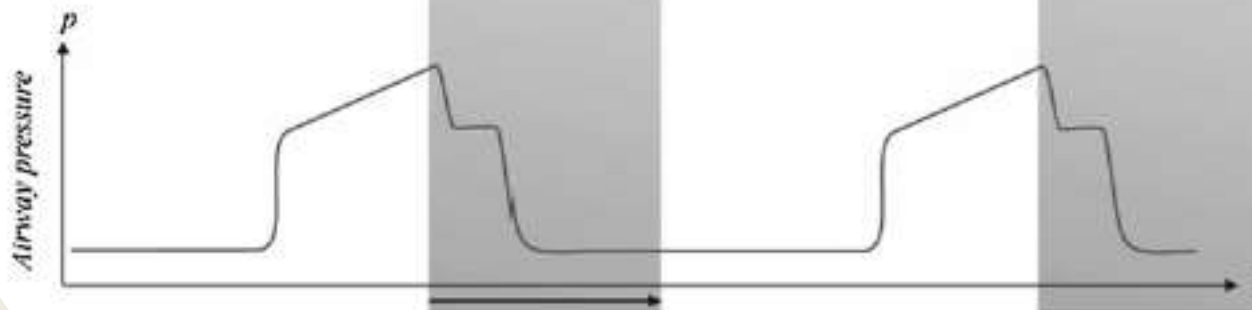
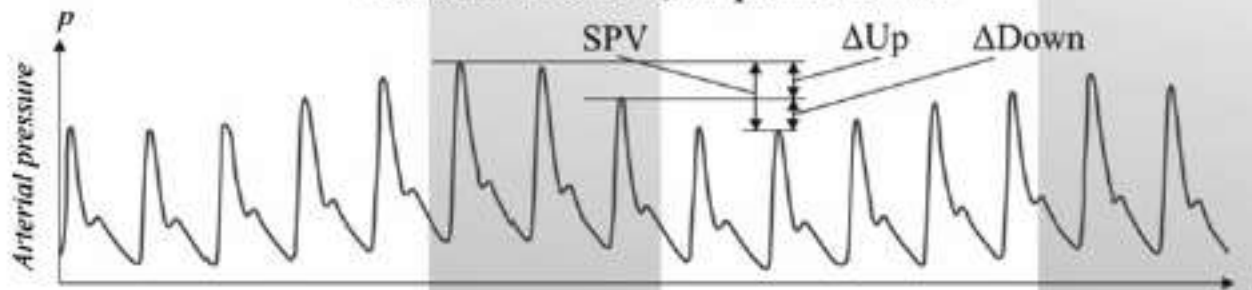
Ventricular end-diastolic volume



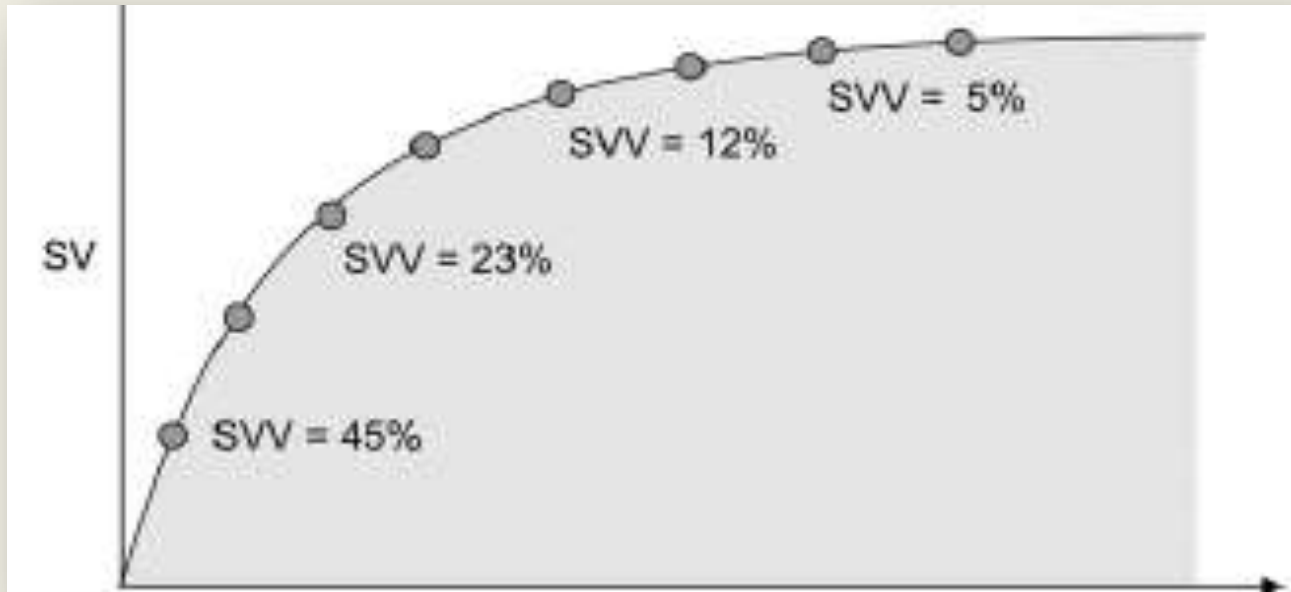
Assessment of SVV and PPV



Assessment of SPV, ΔUp and $\Delta Down$



SVV



Assessing the Diagnostic Accuracy of Pulse Pressure Variations for the Prediction of Fluid Responsiveness

A "Gray Zone" Approach

%9-13 gri zon

Hastalarin %25 i

Limitasyonlar

Spontan solunum

Solunum gayret-Tetik

Aritmiler

Düşük TV (cut of %6,5)

Limitasyonlar

Kompliyans $30 \text{ ml cmH}_2\text{O}$ altında ise

ARDS yanlı negatif restriktif strateji

Yüksek frekanslı ventilasyon

$\text{KH/SS} < 3,6$

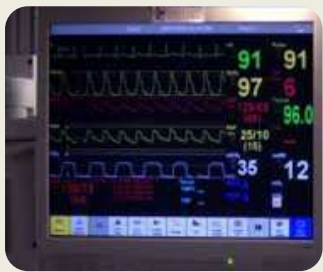
Limitasyonlar

Artmış intraabdominal basınç

Yüksek cut-off

Açık göğüs

SVV-PPV?



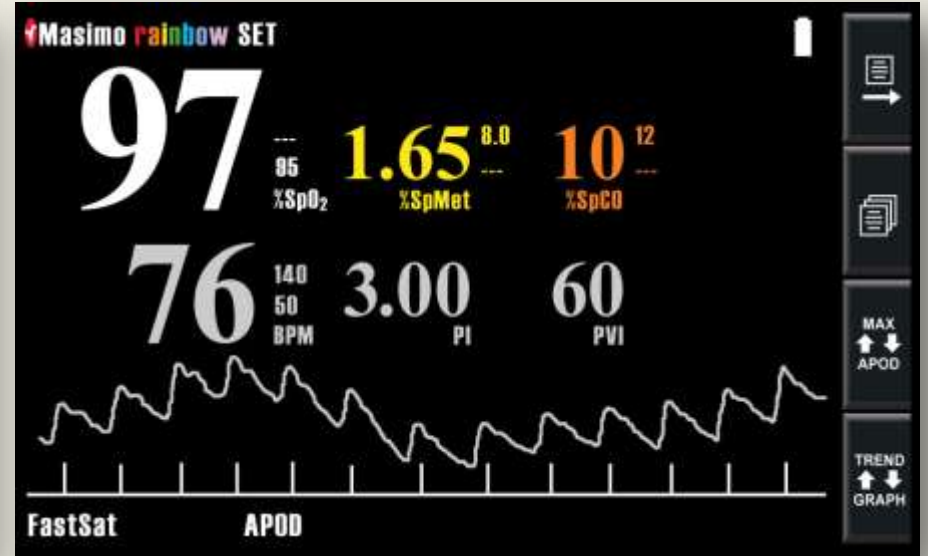
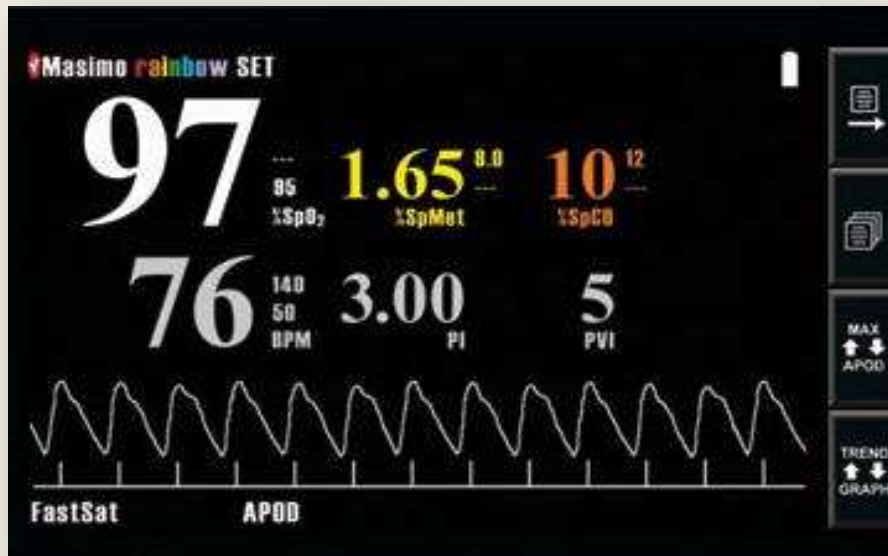
J Clin Monit Comput (2015) 29:197–200

DOI 10.1007/s10877-014-9598-y

LETTER TO EDITOR

Fluid responsiveness is about stroke volume, and not pulse pressure Yogi: the power of Doppler fluid management and cardiovascular monitoring

Pletismografik değişiklikler



Limitasyonlar

GA-MV-Tetikleme yok

Aritmi yok –variabilite yok

TV 8 ml-PEEP 5

Vazomotor tonus (NE-Ağrı-Şok-Vücut sıcaklığı)

Hasta hareketi-sinyal kalitesi

End expiratuvar oklüzyon testi

ARDS de daha güvenli

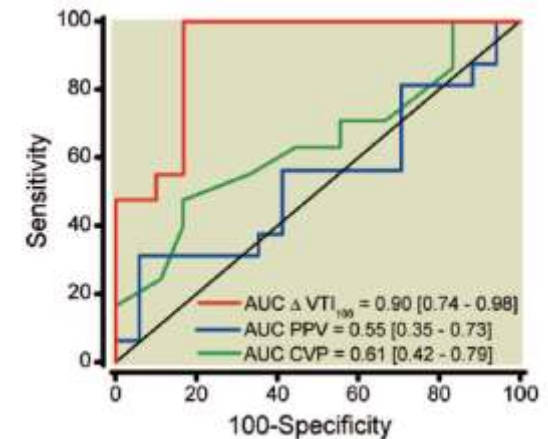
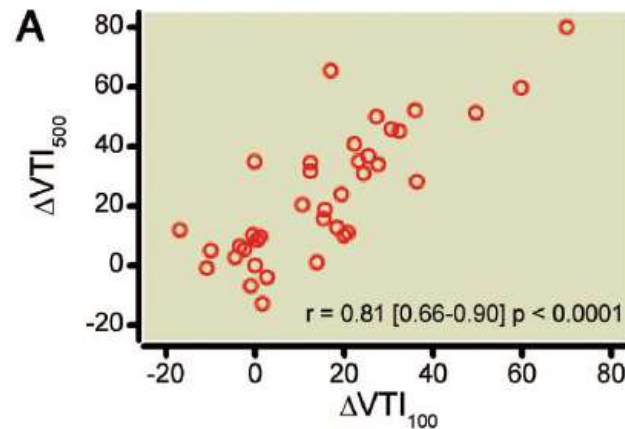
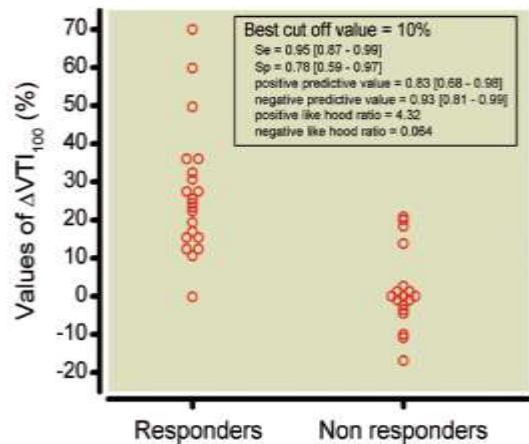
Spontan gayret tetiklerse işe yaramaz

Mini sıvı yükleme (fluid challenge)

An Increase in Aortic Blood Flow after an Infusion of 100 ml Colloid over 1 Minute Can Predict Fluid Responsiveness

The Mini-fluid Challenge Study

- 39-MV-Yb hastası
- Subaortic VTI - TTE
- 100 ml HES 1 dk., 400 ml HES 14 dk., VTI 100



RESEARCH

Open Access

A 10-second fluid challenge guided by transthoracic echocardiography can predict fluid responsiveness



EKO



50-ml kristaloid 10 saniye, 450 ml kristaloid 15 dk.



SV, aortic velocity time index (VTI), and left ventricular ejection fraction (LVEF)

Limitasyonlar

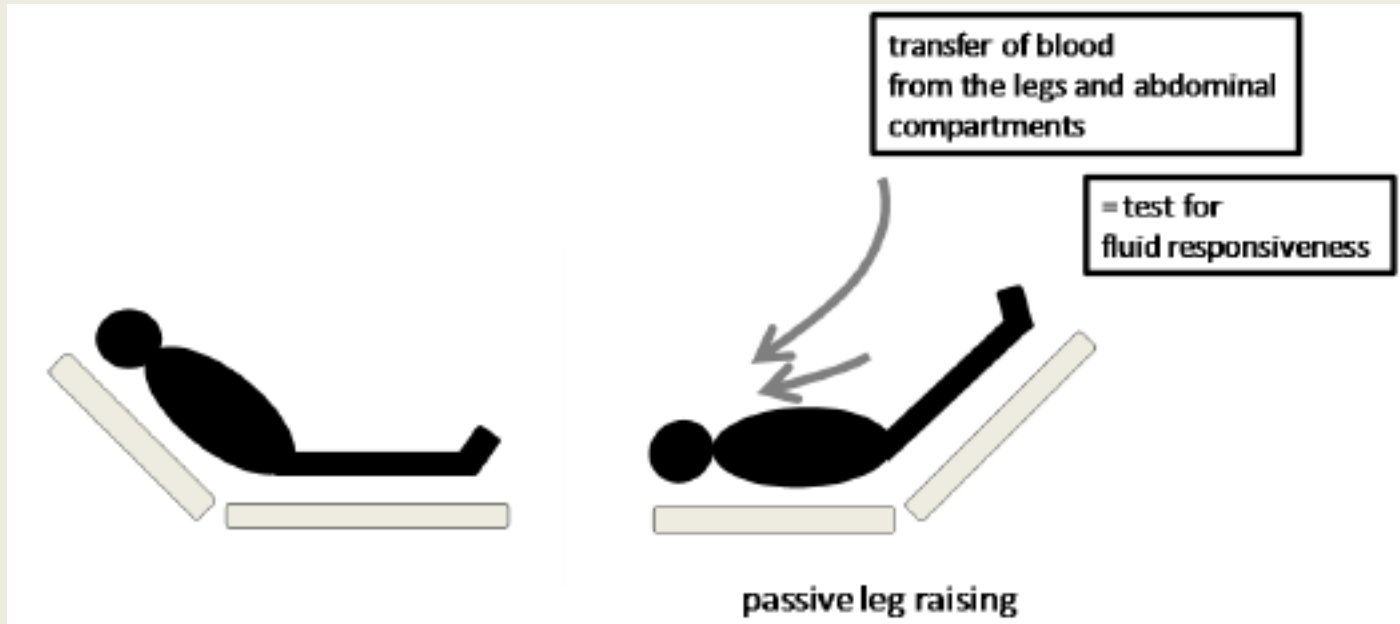


Mini sıvı-Mini
deęişiklik



Keskin bir yöntem

Pasif bacak kaldırma





CI 2.1 \rightarrow 2.6 $\Delta \geq 15\%$
ETCO₂ 32 \rightarrow 37 $\Delta \geq 5\%$

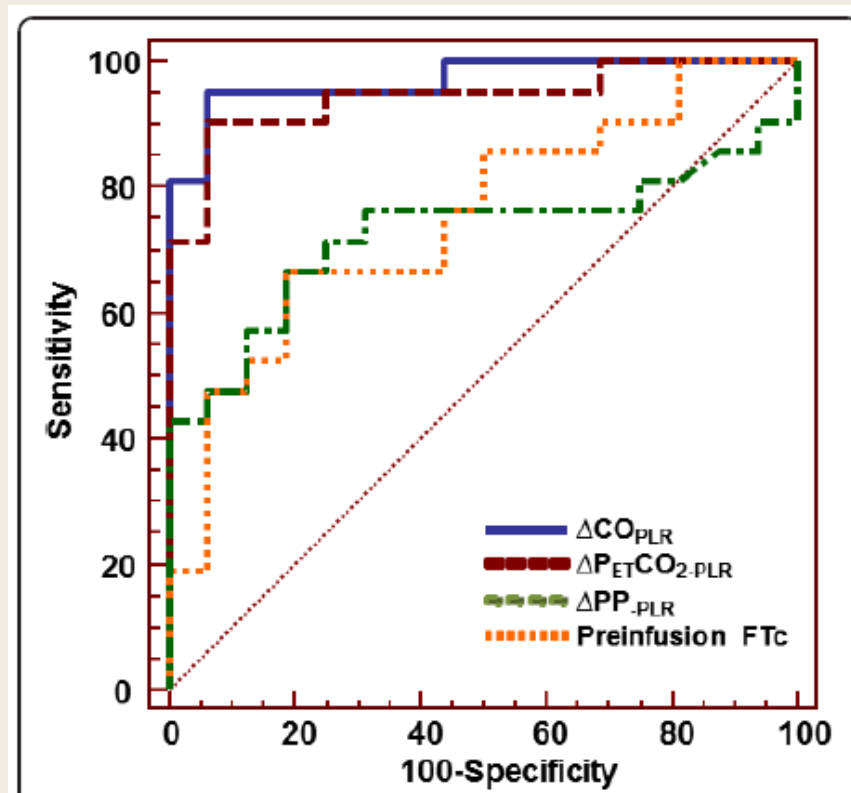


CI 2.1 \rightarrow 2.3 $\Delta \leq 15\%$
ETCO₂ 32 \rightarrow 32 $\Delta \leq 5\%$

RESEARCH

Open Access

Non-invasive assessment of fluid responsiveness by changes in partial end-tidal CO₂ pressure during a passive leg-raising maneuver



Fabio Cavallaro
Claudio Sandroni
Cristina Marano
Giuseppe La Torre
Alice Mannocci
Chiara De Waure
Giuseppe Bello
Riccardo Maviglia
Massimo Antonelli

Diagnostic accuracy of passive leg raising for prediction of fluid responsiveness in adults: systematic review and meta-analysis of clinical studies

Ventilasyon modundan bağımsız



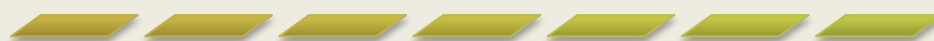
Kardiyak ritimden bağımsız



Teknikten bağımsız



Rutin



PLR cCO > PLR cPP



Limitasyonlar

Her hastaya uygulanabilir mi? Ampute hasta

Her ameliyatta uygulanabilir mi?

İntra abdominal basınç

İntrakraniyal basınç

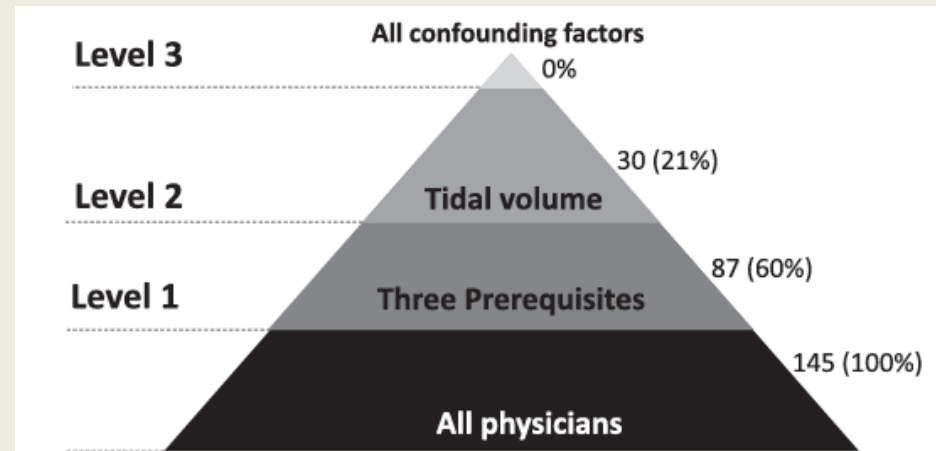


Original article

Evaluation of the knowledge base of French intensivists and anaesthesiologists as concerns the interpretation of respiratory arterial pulse pressure variation

Table 1
Expected answers to clinical cases.

Item	Expected answer
PPV formula	$100 \times \frac{[(PP_{max} - PP_{min}) / ((PP_{max} + PP_{min}) / 2)]}{}$
PPV physiological support	Respiratory variability of arterial pulse pressure
PPV threshold value	> 13%
Gray zone approach	Area of uncertainty without clinical application
PPV prerequisites	Sinus rhythm, controlled ventilation without spontaneous breathing and continuous arterial pressure monitoring
PPV confounding factors	
Respiratory conditions	Vt ≥ 8 mL/kg, HR/RR > 3.6, low respiratory system compliance (< 30 mL/cmH ₂ O) due to low pulmonary compliance
Cardiac conditions	Absence of RVD (TAPSE > 15 mm)
Abdominal conditions	Absence of intra-abdominal hypertension (< 16 mmHg)



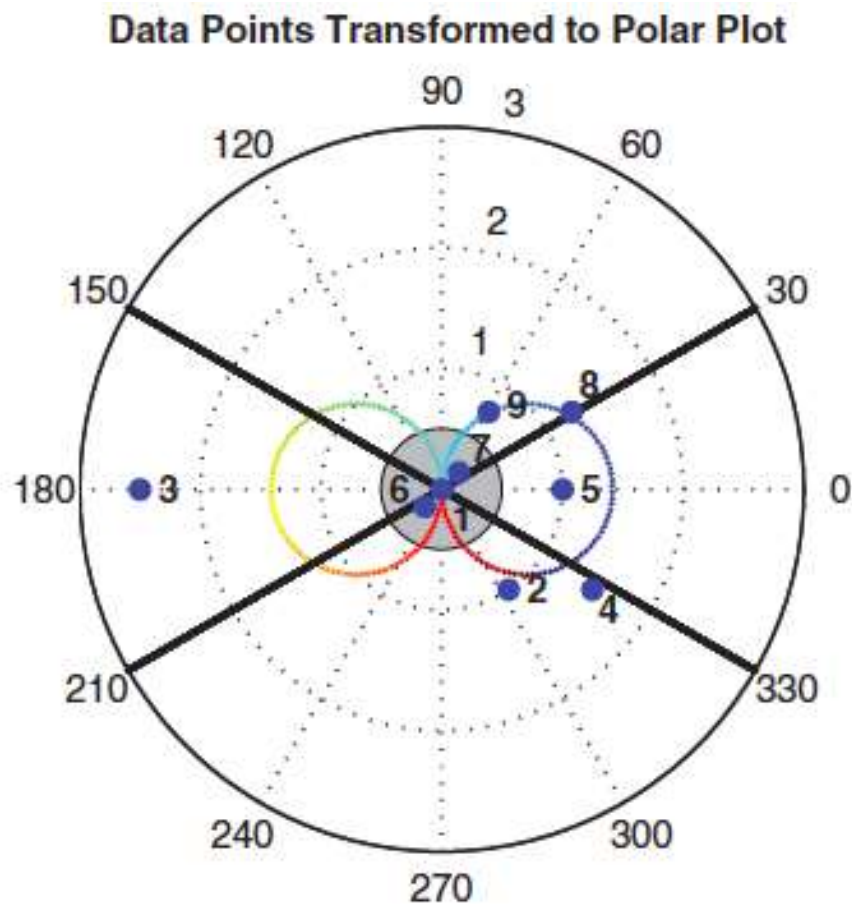
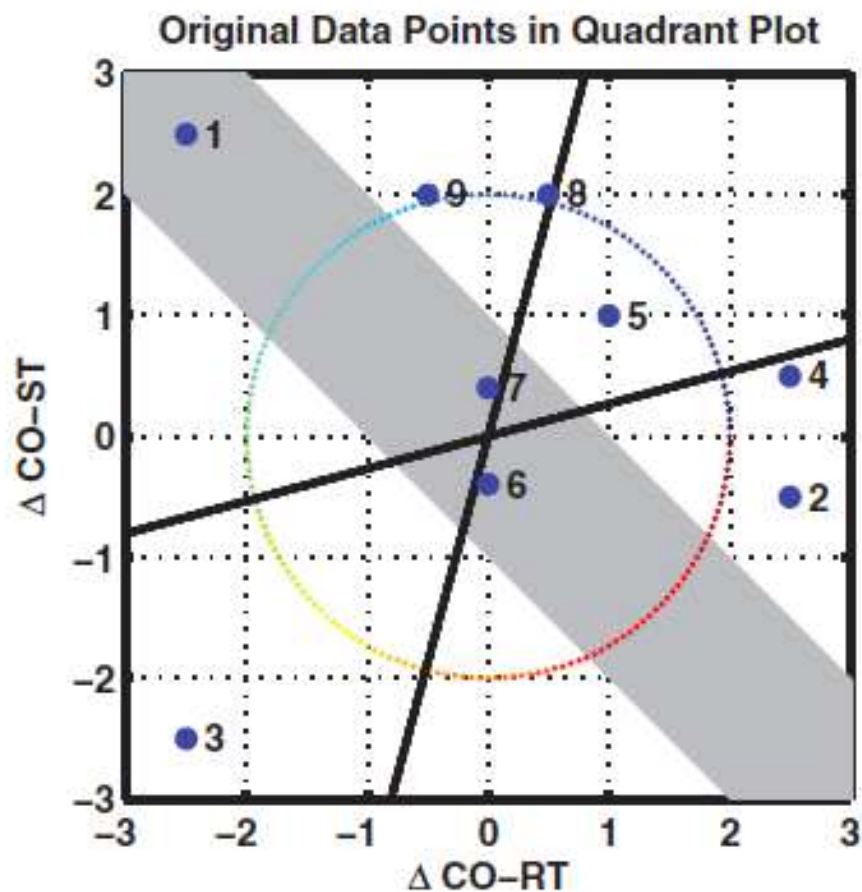
CRITICAL CARE

Evaluation of pulse pressure variation validity criteria in critically ill patients: a prospective observational multicentre point-prevalence study[†]

Methods. A 1 day, prospective, observational, point-prevalence study was performed in 26 French intensive care units (ICUs). All patients hospitalized in the ICUs on the day of the study were included. The ΔPP validity criteria were recorded prospectively and defined as follows: (i) mechanical ventilation in the absence of spontaneous respiration; (ii) regular cardiac rhythm; (iii) tidal volume ≥ 8 ml kg^{-1} of ideal body weight; (iv) a heart rate/respiratory rate ratio > 3.6 ; (v) total respiratory system compliance ≥ 30 ml $\text{cm H}_2\text{O}^{-1}$; and (vi) tricuspid annular peak systolic velocity ≥ 0.15 m s^{-1} .

Results. The study included 311 patients with a Simplified Acute Physiology Score II of 41 (39–43). Overall, only six (2%) patients satisfied all validity criteria. Of the 170 patients with an arterial line in place, only five (3%) satisfied the validity criteria. During the 24 h preceding the study time-point, fluid responsiveness was assessed for 79 patients. ΔPP had been used to assess fluid responsiveness in 15 of these cases (19%).

Tracking Changes in Cardiac Output: Statistical Considerations on the 4-Quadrant Plot and the Polar Plot Methodology



Noninvasive Hemodynamic Monitoring Devices

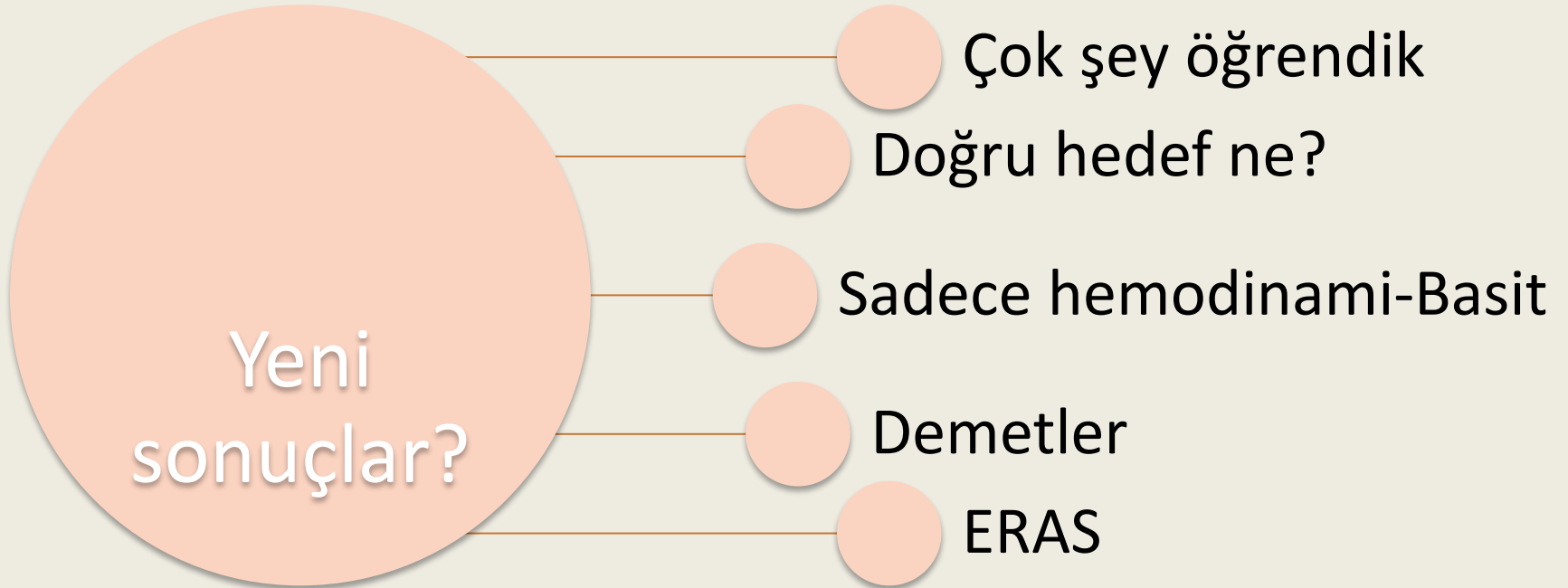
New Tools or Just Another Toy?

Bizim için bulunan bizim bulmadığımız aletler



Goal-Directed Therapy: Time to Move on?

Maurizio Cecconi, MD, FRCA, MD(UK), FICM, and Andrew Rhodes, FRCP, FRCA, FFICM, MD



Hiçbir monitör tek başına outcome

Monitor ihtiyacı zamanla değişir

Herkeseye uygulanacak optimal hemodinamik değer yok

Verilerin kombinasyon ve integrasyonu

Tahmin edilen ölçülen değil

Tek olay non invaziflik değil

Hastanın tipi, sorulan soru, içinde bulunan durum











